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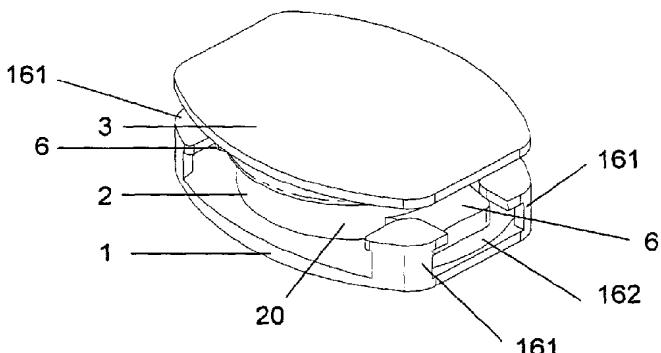
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(54) Title: INTERVERTEBRAL DISC PROSTHESIS AND FITTING TOOLS



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(57) Abstract: The present invention concerns an intervertebral disc prosthesis designed to be substituted for fibrocartilaginous discs ensuring connection between the vertebrae of the vertebral column or the end of the latter. The invention increases stability of such a prosthesis by providing a translation or rotation stop to its nucleus (2), or inducing an angular correction between its plates (1, 20) in contact with vertebrae, or a combination of these characteristics. Such a stop is obtained by parts (6, 20) external to the nucleus, and using contact surfaces perpendicular to their contact directions. Such a stop allows a better stability together with the enforcement of such an angular correction, induced by an angle (A3) between loadbearing surfaces (21, 23) of the nucleus.

## INTERVERTEBRAL DISC PROSTHESIS AND FITTING TOOLS

The present invention concerns an intervertebral disc prosthesis designed to be substituted for fibrocartilaginous discs ensuring connection between the vertebra of the vertebral column or the end of the latter.

The intervertebral discs are formed from a deformable but noncompressible element called "nucleus pulposus" containing approximately 80% water, surrounded by several elastic fibrous layers converging to maintain the nucleus, absorb part of the forces applied to the entire disc and stabilize the articulation. These elements may often be broken down or damaged by compression, displacement or wear and tear, following shocks, infections, exaggerated forces or simply over time.

The breakdown of this articulation element may cause intense pain and significant constraint in the patient. Beyond the surgery that consisted of blocking the deficient articulation and possibly purely and simply removing the damaged disc, a therapeutic route for the last twenty or so years consists of surgically replacing the defective disc with a functional prosthesis. However, the use of such a prosthesis requires a device that is not very cumbersome, that supports significant forces, or has a great sturdiness over time. Furthermore, the comfort of the patients already affected by great and acute pain makes it desirable to arrange for a prosthesis that most faithfully reproduces the natural possibilities of movements and at the same time ensures the best stability possibility to the spinal column that is sometimes already damaged.

The use of such a prosthesis therefore crucially depends on the stability that it allows the spinal column, as much during movements as during static forces or lengthy constant position.

A certain number of prostheses have been proposed with a compressible material base, with the goal of reproducing the kinematics of natural movement while reproducing its components and their characteristics

of shape or plasticity, as described in the patent FR 2 124 815 which proposes a disc from elastomer material reinforced by a textile material. These devices present the drawback of a lifetime that is often too limited and also suffer from drawbacks indeed due to this elasticity. In fact, since the 5 prosthesis is entirely compressible, a progressive sliding of the prosthesis may be produced relative to the vertebra between which it is placed, which too often leads it to leave its housing. The addition of anchoring pins does not allow sufficient remedy for this problem, because the micromovements permitted by the compressibility of the material of the prosthesis also include 10 a vertical component, which too easily allows the pins to leave their housing with each movement.

Among the prostheses nor resting on the deformation of materials, a type of prosthesis frequently used is described by the patent DE 30 23 353 and is formed of a nucleus with the shape of a biconvex lens forming 15 articulation between two plates each presenting a cavity with a shape approximately complementary to the nucleus in their centre and on their perimeter a shoulder retaining this nucleus. This arrangement presents the advantage by comparison to a more limited ball-and-socket joint of using significant contact surface, which largely decreases the wear and tear.

20 To incline one with the other on one side, the plates are articulated by their internal cavity on the edge of the nucleus of the side in question, but according to a rotation movement which, on the other side makes their edges move apart more than they were at rest. This separating has a tendency to detach the vertebral plates on which they are supported, which 25 damages the surface of the vertebra at the sites where the plates have just anchored and again allows progressive displacement with risk of complete ejection of the prosthesis.

Another type of prosthesis described in patent FR 2 659 226 consists 30 of an upper plate presenting a concave face that comes to slide on a nucleus in the form of a segment of a sphere, this nucleus being immobilized in a

cavity of the lower plate. In this case, the rotation is done more satisfactorily from the point of view of space of the plates, but the sliding of the upper plate on a sphere whose centre is located on the exterior of the prosthesis also causes lateral displacement which may be harmful as much to the 5 kinematics of movement as to the organs present in the vicinity.

A solution is proposed in the patent FR 2 730 159 in the form of a nucleus presenting two spherical faces, oriented in the same direction, and with different radius. The nucleus with cylindrical exterior slides on a convex surface belonging the lower plate and itself presents a convex surface on the 10 top, on which the upper plate slides. Because the nucleus is movable horizontally, it is in a position to move apart from one side when the plates approach the other. However, this device presents the drawback of risking the complete ejection of the nucleus outside the prosthesis, this drawback also existing in the device described by the patent DE 30 23 353.

15 In the goal of limiting the risks of ejection of the nucleus, the patents WO 00 53 127, as well as US 5 401 269 and US 4 759 766 propose to provide a translation stop, produced in different ways.

In certain variants, a translation stop is disclosed in the form of a relief protruding from one contact surface of the nucleus and movable in a recess 20 in the plate or inversely. This type of internal stop is therefore located on the interior of a contact or support surface between nucleus and plate, and therefore decreases the available surface considerably. This decrease in support surface increases the stresses undergone by the materials, therefore the risks of wear and tear or strain in creep or exceeding elastic limits. The 25 separation between the support surface and housing receiving the stop may also risk marking the piece which is supported above and damaging the latter.

In certain cases, such a central stop is provided with a noncircular shape, which in a certain extent allows the rotations of the nucleus to be 30 limited relative to the plate that provides it. However, this noncircular forms

additional constraint which again limits the surface available for support. Furthermore, the angles of this shape themselves form fragile zones, which only ensures low sturdiness to this stop operation in rotation.

In other variants, a collar protrudes from the nucleus and surrounds it  
5 in the space between the two plates. In its exterior part this collar widens at a certain height along the axis of the spinal column towards each of the plates, which forms two interior borders that may be supported on the exterior border of contact surfaces of these same plates. However, this type of external peripheral stop presents certain drawbacks, in particular in terms of  
10 obstruction.

In fact, the configuration of this collar represents considerable vertical obstruction (along the spinal column axis) and the contact surfaces of the plates must also present a certain height to be able to stop this collar in translation. Furthermore, the peripheral shape of this type of stop also  
15 occupies considerable radial space, in particular in a section plane where the spinal column presents the smallest width, as in sagittal plane. Given the limited space available in the disc, or intervertebral, space, this obstruction may occupy a space that would be useful for the configuration of the rest of the prosthesis, which may limit the results in terms of kinematics or reliability.

Moreover, this type of external peripheral stop requires a nucleus with biconvex shape to be used, to allow for provision of sufficient height for the contact surfaces of the plates to form an exterior border usable by this stop. Therefore, this type of stop is difficult to produce for a nucleus presenting one or more concave surfaces, while such forms of nucleus may allow the  
25 kinematics of the prosthesis to be made more comfortable with use by the patient.

In the case where the contact surfaces between nucleus and plates are not circular, such a collar may also be able to limit the clearance in rotation of the nucleus relative to the plates, for example by peripheral contact between two concentric ellipses and with different radii. However,  
30

such contact is done according to a very tight angle between the surfaces being supported on each other, which makes the position of this limit not very precise and increases the risks of wear and tear or blockage by clamping. Furthermore, the clearance in rotation permitted by such 5 kinematics is directly dependent on the clearance permitted in translation, and may not be chosen independently of the latter during design of the prosthesis.

A goal of the invention is to propose a prosthesis allowing the spinal column better stability by a greater precision and sturdiness in relative 10 positions of pieces that compose it.

This goal is reached by a vertebral prosthesis device according to claim 1.

Moreover to ensure stability of the spinal column after fitting such a prosthesis, the damages undergone by the spinal column because of the 15 different pathologies leading to deciding to fit a prosthesis sometimes make useful the re-establishing of stability or posture that the elasticity of the spinal column no longer allows to be provided. According to the pathologies and the history of the patient, it may then be indicated to induce a certain angular correction in the configuration of the intervertebral space for example in the 20 sense of lordosis or that of kyphosis.

Certain types of existing prostheses use a variation in thickness of one of the plates to induce such a correction. Such a correction is not however always very stable, in particular because the position of supports of the nucleus on the plates varies too much during movements.

25 Another goal of the invention is therefore to propose a prosthesis allowing the prosthesis better stability by the re-establishment of posture adapted to the kinematics of movements that it produces.

This goal is reached by a vertebral prosthesis device according to claim 5.

Additional developments of the invention are described in the dependent claims.

The invention with its characteristics and advantages will be more clearly evident with reading the description made in reference to the attached drawings in which:

- Figure 1 represents an exploded view in perspective of a prosthesis according to the invention, in a version including a convex lower plate and providing a central and annular stop;
- Figure 2 represents an exploded sectional view of a prosthesis device according to the invention in the same variant;
- Figure 3 represents an exploded sectional view of the prosthesis device according to the invention in a variant including a nucleus with flat lower surface and lower plate presenting an annular stop;
- Figure 4 represents an exploded sectional side view of the prosthesis device according to the invention in a variant including a nucleus with concave lower face, an added block and a lower plate with annular stop;
- Figure 6a represents a sectional side view of the prosthesis device according to the invention in a variant with central, annular and incline stop, in maximum incline position;
- Figure 6b represents a sectional side view of a prosthesis according to the prior arts where the nucleus presents a fixed position;
- Figure 6c represents a sectional side view of a prosthesis according to the prior arts where the nucleus is movable and is ejected under the load during a force in the maximum incline position;
- Figure 5 represents a sectional exploded side view of the prosthesis device according to a variant including an added block allowing a central stop to appear and a flat lower plate presenting an annular stop;
- Figure 7 represents a sectional side view of the prosthesis device according to a variant without annular stop and where the central stop

presents a vertical section in the form of a dovetail, in maximum incline position;

- Figures 8a and 8b represent sectional side views of the prosthesis device according to the invention according to a variant with inclined axis, 5 including an annular stop and a central stop incorporated in the contact surface supporting the nucleus, in the case of a single piece lower plate and an added block, respectively.
- Figure 8c represents a sectional side view in a sagittal plane of the prosthesis device according to the invention according to a variant with a corrective nucleus presenting two faces in which the contact surfaces are not parallel; 10
- Figure 9a represents a perspective view of the prosthesis device according to the invention according to a variant with two stops exterior to the nucleus, held in a housing between pillars integral with the lower plate;
- Figure 9b represents a perspective view of the prosthesis device according to the invention according to a variant with two stops exterior to the nucleus, each holding a pillar integral with the lower plate between its arms; 15
- Figure 10 represents a perspective view of a device according to the invention for fitting such a prosthesis; 20
- Figure 11 represents a perspective view of a device according to the invention for inserting such a prosthesis, in position during the introduction laterally of the prosthesis between two vertebrae;
- Figure 12 represents a perspective view of an assembly tool with an insertion guide according to an embodiment of the invention; 25
- Figure 13 represents a perspective view of a prosthesis according to the invention, presented at the entrance of the insertion guide of the invention;

– Figure 14 represents a perspective view of the instrumentation according to an embodiment of the invention when the prosthesis is ready to be impacted in the disc space.

A prosthesis according to the prior art disclosed by the patent FR 2 659 226, consisting of a concave upper plate (3AA) sliding on a nucleus (2AA) presenting a spherical upper cap (23AA) itself immobilized in a housing of the lower plate (1AA), is represented in Figure 6b; in horizontal position and in maximum incline position. Because the centre of the sphere (csAA) providing the contact surface with the nucleus is located outside this same upper plate (3AA), its incline is combined with considerable lateral displacement (dl). This displacement creates a break in the continuity of the vertical profile of the vertebral column which may hamper the overall functionality of the movement and risk damaging the tissues surrounding the vertebrae, such as ligaments and spinal marrow, which may be immediately or in the long run.

A prosthesis according to the prior art disclosed by the patent FR 2 730 159, represented in Figure 6c, consists of a movable nucleus with two spherical surfaces oriented in the same direction, that may be laterally displaced between two plates and may allow incline without lateral displacement. In the extreme position, however, the nucleus is only kept on the exterior side by the furthest border of the spherical surface of the upper plate. Since this edge itself is already raised, there is a great risk that too high a vertical pressure or a horizontal parasitic force causes ejection of the nucleus towards the exterior of the prosthesis, causing intense pain and risks of immediate damage for the tissues surrounding the vertebral column, such as ligaments or spinal marrow.

In an embodiment represented in Figure 6a, a prosthesis according to the invention consists of a lower plate (1) being articulated with an upper plate (3) around a nucleus (2) presenting two spherical sliding surfaces with the same orientation on both faces. The lower surface (21) of the nucleus (2)

is concave and slides on a complementary convex surface (12) provided by the upper face, known as internal, of the lower plate (1). The upper surface (23) is convex and slides on a complementary concave surface (32) provided by the lower face, known as internal, of the upper plate (3). In this 5 embodiment, the radius of the lower contact surface (21) of the nucleus (2) is a radius greater than that of its convex upper surface (23), the centres of the spheres providing its two contact surfaces being located on the same axis of symmetry (d2) of these two surfaces. On their side, the two plates present contact surfaces (12, 32) the axes of symmetry (d12, d32) of which are 10 perpendicular to their external faces (10, 30). The horizontal displacement part of the nucleus in one direction, due to the rotation on the upper sliding surface around its centre (cs), is compensated by a rotation of the nucleus on its lower sliding surface around its centre (ci) which induces horizontal displacement of the nucleus (2) and therefore of the centre (cs) of the upper 15 sliding surface. The radii of the two spheres providing these sliding surfaces (12, 21, 23, 32) are determined so as to modify the lateral displacement of the plates by comparison with each other during their incline. In one embodiment, the radii of these sliding surfaces (12, 21, 23, 32) may be chosen so that the movement of the plate is reduced to an incline 20 accompanied with a possible vertical component but without horizontal displacement of the upper plate relative to the lower plate.

To avoid any risk of ejection of the nucleus (2) during forces in the inclined position, the latter is kept in its clearance by a central stop, formed for example by a cylindrical block (4) protruding from the convex surface of 25 the lower plate and cooperating with edges of a recess (22) arranged in the centre of the contact surface (21) of the lower concave surface of the nucleus.

In one embodiment (Figure 6a) the lower plate also presents on its upper face an approximately cylindrical cavity (11) in which the edges (112) 30 protrude from the contact surface (12) with the nucleus (2), and cooperate

with the approximately cylindrical perimeter (20) of this nucleus to ensure an operation of annular stop for it while limiting its movement towards the exterior of the contact surface (12) that provides it.

In one embodiment (Figure 6a) the internal surfaces of the plates, on 5 their parts (113, 331) exterior to the sliding surfaces, present a form capable of cooperating among themselves to limit by stop the incline of the plates with each other at a determined angle (a1).

In one embodiment represented in Figure 7, the stop (4) is provided by the convex surface (12) of the lower plate (1) and presents approximately 10 the shape of an inverted cone, that is, its section is greater in its end (42) opposite the surface (12) that provides it. By presenting an undercut shape, the interior surface (224) of the recess (22) cooperates with the exterior surface (40) of the stop (4) to limit the raising of the nucleus when the latter is in furthest position against this stop (4).

15 According to the criteria connected for example to the resistance of the materials, to the wear and tear or to the kinematics sought, the different shapes and dimensions intervening in the stop mechanisms, for example exterior (Figures 9a and 9b), annular, central or incline, could be determined so as to coordinate the order of arrival at stop of the different parts. These 20 shapes and dimensions could be determined for example, so that the pieces reach stop at the same stage of movement, for example determined by angular incline (a1) between the lower (1) and upper (3) plates.

In an embodiment illustrated in Figure 7 and 8a, the annular stop operation is used very little or not at all, which allows the vertical obstruction 25 of the prosthesis to be decreased.

In an embodiment presented in Figure 3, the lower surface (21a) of the nucleus (2) may be approximately flat, and then slide on a contact surface (12a) of the lower plate (1), also approximately flat. In this embodiment, the flatness of the contact surface (12a) of the lower plate 30 allows the edges (112) of this plate that protrude from this surface to be

particularly effective in their role of annular stop. Therefore, it is possible to manage without the central stop and thus to increase the common contact surface between the lower plate and the nucleus, which on the one hand, decreases the wear and tear of the pieces and on the other hand, the risk of 5 marking the surface of the plate with placement of the contour of the recess (22, Figure 6a) in which is accommodated the central stop (4, Figure 6a) in other embodiments.

In an embodiment represented in Figure 4, the lower plate (1) presents an approximately cylindrical cavity (11) on its upper face the flat bottom (15) of which receives an intermediate piece called block (5). This piece is immobilized in the cavity (11) for example by the edges (112) of this cavity and presents on its upper face a convex surface (52) on which the lower concave surface (21) of the nucleus slides. This embodiment with the convex surface (52) on which the nucleus slides for example allows the good 10 qualities of the surface necessary for the fluidity of movement and longevity of the prosthesis to be obtained more easily and at less cost. It also allows several models to be provided with blocks (5), of different shapes or qualities, that can be chosen in advance or at the time of the surgery 15 according to applications with the same model of lower plate.

20 In an embodiment represented in Figure 5, the lower plate (1) receives a block (5) in an approximately cylindrical cavity (11) presenting a vertical perforation that the stop (4) integral with the lower plate crosses. On its upper surface, this block supports a convex surface (52), on which the nucleus (2) and upper plate stack rests.

25 As a variant, the stop (4) may be integral with the block (5) on its convex contact surface (52)(Figure 8b).

Within the goal of obtaining at rest a corrective effect of the relative position of two vertebrae, the prosthesis may be produced in a variant where the axes of symmetry of the contact surfaces (12, 15, 52, 21, 23, 32) or 30 support (10, 30) of one or more pieces are not merged. The pressure (F)

exerted by the vertebrae on the two plates in the directions perpendicular to their external surfaces (10, 30) will then have the tendency to induce and continuously maintain an incline (a3, Figures 8a, 8b et 8c) between these plates (1, 3), that is not zero, for example in the sense of lordosis.

5 An embodiment of such a variant is represented in Figure 8a where the axis of symmetry (d12) of the contact surface (12) of the lower plate (1) forms an angle (a2) determined with a direction (d10) perpendicular to the external surface of this same lower plate, while the axis of symmetry (d32) of the internal contact face (32) of the upper plate (3) is perpendicular to the  
10 external surface (30) of this same upper plate (3). The lower contact surface of the upper plate (3) presents an axis of symmetry parallel to a direction perpendicular to the support surface (30) of the external face of this same upper plate (3).

In another variant according to the same principle represented in  
15 Figure 8b, a device is used that includes a lower plate (1) providing a block (5) the upper contact surface of which (52) presents an axis of symmetry (d52) forming an angle (a2) determined with a direction (d51) perpendicular to its lower face (51). The internal contact surfaces (15, 32) of the lower (1) and upper (3) plates present axes of symmetry perpendicular to the support  
20 surface (10, 30) of their respective external faces. Thus, at the time of the surgery it is possible to choose between several blocks (5) with different inclines, according to the desired degree of correction. This block (5) could be maintained fixed around an axis perpendicular to the lower plate (1) by any known means (not represented) such as wedge, grooves or  
25 complementary accidents of shape between the block (5) and the lower plate (1) that provides it.

In another variant according to the same principle, represented in Figure 8c, it is the nucleus (2) that presents two contact surfaces (21, 23) the axes of symmetry of which (d21, d23) form a determined angle (a2) between them. The internal contact surfaces (12, 32) of the lower (1) and upper (3)

plates present axes of symmetry perpendicular to the support surface (10, 30) of their respective external faces. The angular correction (a3) induced by the nucleus (2) could then be kept constantly in the desired direction relative to the body of the patient by a rotation stop mechanism (not represented in 5 Figure 8c) of this same nucleus, such a mechanism being described later (Figures 9a and 9b).

In one embodiment the device according to the invention presents an exterior stop mechanism, located outside the perimeter of the contact surfaces of the nucleus (2).

10 In a variant represented in Figure 9a, this mechanism is formed of two protruding parts (6) protruding from the cylindrical exterior surface of the perimeter of the nucleus (2) in opposite directions. Each of these protruding parts is held in a housing (162) delimited by two pillars (161) integral with the lower plate (1). These pillars cooperate with the protruding part (6) or with 15 the surface (20) of the perimeter of the nucleus or both for limiting the movements of this same nucleus in translation as in rotation parallel said plate. The housing is sufficiently large to allow small displacements of the nucleus required for the kinematics of the device, while being sufficiently narrow so that this same nucleus and the lower plate are adjacent in certain 20 positions, for example, positions of maximum incline of the spinal column. The protruding part (6) or perimeter surface (20) of the nucleus (2) then cooperates with the pillars (161) of the lower plate to retain this same nucleus and avoid any lateral ejection.

The pillars (161) present a larger section at the end than at the base, 25 thus limiting the raising of the nucleus.

In another operating variant according to the same principle and represented in Figure 9b, this mechanism is formed of two protruding parts (6) protruding from the cylindrical exterior surface (20) of the perimeter of the nucleus (2) in opposite directions. Each of these protruding parts presents 30 two arms delimiting a housing (66) which hold a pillar (163) integral with the

lower plate (1). The pillars (163) present a larger section at their end than at their base.

These embodiments of stop (9a and 9b) may allow the central stop to be disposed of and to thus increase the contact surfaces which decreases  
5 the wear and tear. These types of stop (6) are also particularly valuable because of the limitation of the movements of the nucleus in rotation along an axis approximately parallel to the axis of the spinal column. In fact, this limitation makes it possible to use a corrective nucleus in which the contact surfaces present axes of symmetry that are not parallel, while maintaining in  
10 them the correction in a constant direction relative to the body of the patient.

In an embodiment represented in Figure 6a, the lower (1) and upper (3) plates receive means for bony anchoring on their external face, designed to immobilize the prosthesis between the vertebrae or adjacent elements of the spinal column. These anchoring means may be pins (8) or wings presenting a small cross section at their end away from the plate that provides them. These pins then are embedded or are impacted by punching in the material of the bony elements (V) between which the prosthesis is fitted, for example under the effect of the pressure exerted by the ligaments when the tools are withdrawn, the tools that kept the vertebrae separated.  
15 Driving in the pins in the material of the bony element (V, Figure 6) then prevents the prosthesis from sliding outside its site.  
20

In an embodiment represented in Figure 1, the plates (1, 3) present one or more accidents of shape such as notches (7) or perforations (not represented) enabling catching of a grasping tool to remove the prosthesis  
25 from its site in case of need. The lower plate (1) presents a convex upper contact surface (12) providing a central stop (4) and a cavity presenting edges (112) forming an annular stop.

In an embodiment represented in Figure 10, an insertion device according to the invention is presented in the form of an element (9) called  
30 insertion guide, presenting an internal channel (90) approximately

rectangular in section in which the prosthesis (P) can slide. This channel (9) is formed from two semi-guides (91, 92) with a cross section in the shape of a "U", arranged inversely and fitted into each other. At one of the ends, this guide (9) presents one or more parts called support blocks or edges (910, 5 920) protruding along its longitudinal axis (d9). These support blocks (910, 920) form an extension of the walls of the channel called vertical (9) that form the small sides of the rectangular section of the channel (9).

In an application method illustrated in Figures 10 and 11, the fitting of the prosthesis device according to the invention is carried out according to 10 the following steps:

- separating the vertebrae with the aid of known instruments, for example distraction tools;
- sliding the insertion guide (9) around the distraction tools so as to introduce the support edges (910, 920) between the vertebrae (V);
- 15 - release and extraction of the distraction tools, the vertebrae being kept spread apart by the support edges of the insertion guide;
- introduction of the prosthesis ready for fitting into the channel, and sliding to near the spinal column;
- 20 - adjustment of the incline of the prosthesis according to conformation of the space available between the vertebrae with possible separating of the two parts (91, 92) of the channel according to a corresponding angle (a9) to help with this adjustment;
- positioning of the prosthesis in the intervertebral space by pushing by the interior of the channel;
- 25 - extraction of the support blocks (910, 920) of the channel outside the intervertebral space and impacting blocks for bony anchoring in the vertebrae (V).

In an embodiment illustrated in Figures 12a to 14, the instrumentation used for fitting the prosthesis according to the invention comprises an 30 insertion guide (93) provided with an internal channel (90). This channel (90)

presents an approximately rectangular cross section, or with a shape approximately complementary to the exterior profile of the prosthesis. This internal channel (90) is provided with dimensions and shape adequate for allowing the prosthesis to pass and to guide from one of its ends to the other,

5 in a position and along a displacement approximately parallel to the external faces of its plates (1, 3). According to the applications, the channel (90) of the insertion guide (93) may include scallops in its walls opposite plates of the prosthesis. Such scallops make it possible to allow the anchoring means (8, 81) to pass provided by the plates of the prosthesis, while guiding the

10 latter sufficiently precisely in the channel. In the embodiment illustrated here these scallops have the shape of grooves (934, 936) along the axis (d9) of the channel provided by the internal walls of the channel opposite plates (1, 3).

At one of its ends, called the working end, the walls (931, 932) of the

15 channel (90) perpendicular to the plates of the prosthesis, that is, located in the plane containing the axis of the spinal column, are extended along the axis (d9) of this channel over a distance determined so as to protrude relative to the walls of this same channel that are parallel to the plates of the prosthesis. Since these extensions thus form the protruding parts, or support

20 edges, that may be inserted in the intervertebral space to maintain the separation of the plates from the two vertebrae surrounding this space.

The height of these support edges (931, 932) is determined so as to maintain adequate space for allowing the introduction of the prosthesis and its anchoring means (8, 81), according to the method of anchoring provided.

25 If the anchoring means are formed from sockets (8) or wings (81) before being introduced freely in the space, the support edges will have sufficient height to allow the height of these sockets or wings to pass. If the anchoring means are formed from wings having to penetrate the vertebral plates by a hollowed trench in the surface of these plates and opening laterally, the

height of these support edges could be sufficiently low to allow the height of the prosthesis to pass but not the wings.

During surgery for fitting such a prosthesis, the surgeon begins by removing the vertebral disc or its debris, and then uses distraction tools to increase the disc space available between the two vertebrae having to receive the prosthesis. Such tools are often formed with an elongated handle providing a flat part at the end. This flat end is introduced between the vertebrae, then it is made to pivot to increase the separation of the vertebrae.

In the instrument according to the invention, the internal channel (90) of the insertion guide (93) is provided to be able to be threaded around such distraction tools, once they are in place between the vertebrae. Once brought near the spinal column while surrounding the distraction tools, the insertion guide is pushed so as to introduce its edges (931, 932) between the vertebrae, in a plane approximately parallel to the spinal column. The distraction tools may then be removed from the spinal column by making them slide in the channel (90) of the insertion guide, while the height of the support edges preserves sufficient space between the vertebrae to allow fitting of the prosthesis. In the embodiment illustrated here, the insertion guide (93) presents means for interlocking with a guide assembly tool (94), used to bring it near the spinal column and facilitating its fitting. This guide assembly tool (94) is also usable for removing the insertion guide and its support edges, and allowing the vertebrae to tighten on the prosthesis, once the latter is in place.

Such a guide assembly tool (94) is illustrated in Figures 12a and 12b. This tool (94) consists of two elongated tubes (941, 946) articulated to each other by means (945) located at one end, called assembling, of this tool. These two elongated tubes at their end located opposite the assembling end, each provide interlocking means for insertion guide (93). These interlocking means may comprise, for example, a hook (942, 947) on each tube (941,

946) the opening of which is located opposite the other tube. When the guide assembly tool (94) is approached by the insertion guide (93), the fact of tightening the tubes to each other around their articulation makes it possible for each hook (942, 947) to tightly encircle a tongue (934, 936) in the shape 5 of a "T" protruding on each groove (933, 935) of the insertion guide. Within and in the axis of each tube (941, 946) is found a rod (943, 948) that may be displaced longitudinally relative to the tubes by screwing means comprising a screwing wheel (944, 949). The screwing of these wheels causes the advance of the rod in the tube and the end of the rod opposite the screwing 10 wheel then comes to lean and block the tongue (934, 936) of the insertion guide (93) within the hook (942, 947) provided by the tube receiving this same rod. This blockage thus makes it possible to interlock the guide to its assembling tool sufficiently stably to make it possible to position said guide around the distraction tools at the spinal column.

15 These means (934, 936) of interlocking the insertion guide (93) or others provided by said insertion guide also make it possible to guide and interlock means of approach (95) to this insertion guide. These means (95) of approach include means for positioning the prosthesis, these means of positioning being provided to position and maintain the assembled prosthesis 20 in a determined position relative to these means (95) of approach even in the absence of the insertion guide (93). This positioning of the prosthesis on the approach means makes it possible for the interlocking of the approach means and the insertion guide to put the prosthesis in a position making it possible for it to be easily displaced from these same means of approach up 25 to in the internal channel (90) of the insertion guide (93). Thus, it is possible to prepare the prosthesis in the approach means (95) independently of the rest of the operation. Then it is possible to fit the insertion guide on the spinal column without being preoccupied with the prosthesis, then easily and rapidly inserting this prosthesis in the insertion guide (93) while the latter is 30 already in position against the spinal column.

As well as illustrated in Figure 14, these approach means (95) include two shafts (951, 952) connected to each other by articulation (955) so as to come to pinch the prosthesis (P) between two flattened parts ensuring a determined position of the prosthesis relative to these approach means. The 5 ends of these shafts opposite the articulation including interlocking means (953, 954) capable of cooperating with the interlocking means (934, 936) of insertion guide (93) to ensure a determined position of approach means (95) relative to the insertion guide (93) as well as certain stability to this assembly. At the end of each shaft (951, 952), these interlocking means (953, 954) may 10 in particular comprise a scalloping in which the arms come to encircle the exterior of the groove (933, 935) of the insertion guide while gliding under the upper bar of the "T" formed by the tongue (934, 936) provided by this same insertion guide.

Once the insertion guide (93) fitted instead of the distraction tools and 15 the approach means (95) interlocked to this guide, the prosthesis is therefore in a stable position relative to the spinal column, and may be inserted in the insertion guide then slide up to the disc space. This displacement is achievable here with the aid of impacting means, or impactor (96) comprising an impacting end capable of pressing on the assembled prosthesis, 20 distributed on both plates and without touching the nucleus. This impactor includes a central elongated part (960) that can be inserted in guiding means as an opening in the shape of a "U" provided by approach means (95) at their articulated end (955). This impactor includes another end (962) called assembling or striking, that can act to apply a continuous pressure or 25 repeated shocks, with the hand or by any known tool or apparatus. Such an action, applied on the assembling end (962) of the impactor in the axis (d9) of the channel (90) then will be reverberated by the end (961) on the prosthesis, so as to cause its entrance then sliding in the channel (90) of the insertion guide (93), then its insertion or impaction in the intervertebral 30 space.

In all the prosthesis devices according to the invention described here, it is necessary to understand that the distinctions of "lower plate" (represented on the bottom of the figures and referenced 1) and "upper plate" (represented on the top of the figures and referenced 3) are above all 5 conventional, the device being able to be used in a different position, even inverse of that consisting of placing the lower plate toward the bottom of the vertebral column.

Thus, the invention proposes an intervertebral disc prosthesis device comprising at least three pieces, which parts include a plate (1) called lower 10 and a plate (3) called upper (3) producing around at least one intermediate part called nucleus (2) an articulation by support or sliding between loadbearing surfaces (12, 15, 21, 23, 32) of said pieces, one of these pieces including at least one protruding part or accident of shape cooperating with the shape of at least one other of said pieces to form an stop limiting the 15 possibilities of movement of the nucleus, characterized in that this stop operation uses at least one stop external to the loadbearing surfaces comprising at least one part (161, 163) protruding from at least one plate (1), located outside the loadbearing surface (12, 15) of said plate and including a face directed towards the interior of the prosthesis, this face cooperating with 20 a peripheral part (6) of the nucleus (21, 23) situated outside its loadbearing surfaces (21, 23) and in which the surface is directed towards the exterior of the nucleus, to limit displacements of the nucleus in translation or in rotation or both in a plane approximately transverse to the spinal column.

According to a particular aspect, the loadbearing surfaces (21, 25 21a, 23) of the nucleus (2) in contact with the lower plate (1) and upper plate (3) present axes of symmetry (d21, d23, respectively) forming between them a determined angle (a2) that is not zero, so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their external surfaces induces an incline (a3) of these plates with each other.

According to a particular aspect, this external stop limits the movements in rotation of the nucleus (2) relative to at least one plate (1) by contact between parts (6, 161, 163) supporting each other by stop surfaces, this support being done along a direction approximately parallel to the  
5 normal of each of these stop surfaces.

According to a particular aspect, the external stop includes a tongue (6) protruding from the nucleus (6) which cooperates with one of the plates (1) by confining this tongue (6) in a housing (162) delimited by pillars (161) protruding from the internal face of this same plate (1) or by a recess (66)  
10 separating this tongue into two arms encircling a pillar (163) protruding from the internal face of this same plate (1), the internal face of a plate being defined at that oriented on the side of the nucleus.

According to a particular aspect, the end of at least one pillar (161, 162, 163) presents a section greater than its base, this enlargement of the  
15 pillar cooperating with the shape of the external stop tongue (6) of the nucleus (2) to limit the raising of this same nucleus relative to the plate (1) providing this pillar.

In the same spirit, the invention also proposes an intervertebral disc prosthesis device comprising at least three pieces, including a plate (1) called lower and a plate (3) called upper (3) producing around at least one intermediate element called nucleus (2) an articulation by support or sliding between loadbearing surfaces (12, 15, 21, 23, 32) of said parts, one of these parts including at least one protruding part or accident of shape cooperating with the shape of at least one other of said parts to form an stop limiting the  
20 possibilities of movement of the nucleus, characterized in that the loadbearing surfaces (21, 21a, 23) of the nucleus (2) in contact with the lower plate (1) and upper plate (3) present axes of symmetry (d21, d23, respectively) forming between them a determined angle (a2) that is not zero so that a pressure (F) exerted on the two plate (1, 3) along directions  
25

perpendicular to their external surfaces induces an incline (a3) of these plates with each other.

According to a particular aspect this device is characterized in that the operation of the stop uses at least one stop external to the loadbearing surfaces comprising at least one part (161, 163) protruding from at least one plate (1) located outside the loadbearing surface (12, 15) of said plate and including a face directed towards the interior of the prosthesis, this face cooperating with a peripheral part (6) of the nucleus located outside its loadbearing surfaces (21, 23) and in which the surface is directed towards the exterior of the nucleus, to limit the displacements of the nucleus in translation or in rotation or both in a plane approximately transverse to the spinal column.

According to a particular aspect, when the two plates have their external faces (10, 30) parallel to each other, their loadbearing surfaces (12, 12a, 32) cooperate with the loadbearing surfaces (21, 21a, 23) of the nucleus (2) present axes of symmetry (d12, d32) forming a determined angle (a4) between them so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their external faces induces an incline (a5) of these plates with each other.

According to a particular aspect, the loadbearing surfaces (12, 32) provided by the internal face of the lower plate (1) and the internal face of the upper plate (3) are each in complementary contact with a supporting surface (21, 23, respectively) of the nucleus (2), and each present a shape, convex and concave, respectively, or inversely, this nucleus itself presenting a perimeter (20) approximately cylindrical along the axis of symmetry of its contact faces (21, 32).

According to a particular aspect, the internal face of the lower plate (1) presents a loadbearing surface (12a) cooperating with a loadbearing surface (21a) of the lower face of the nucleus (2), this same nucleus including on its upper face a convex loadbearing surface (23) in complementary contact with

a concave loadbearing surface (32) of the internal face of the upper plate (3) the loadbearing surface (12a) of the internal face of the lower plate being sufficiently extended to allow movement of the nucleus relative to this same lower plate.

5 According to a particular aspect, an intermediate element called block (5) is added on the internal face of one (1) of the plates and produces an articulation with the other plate (3) around the nucleus (2) which nucleus presents a concave loadbearing surface (21) and a convex loadbearing surface (23) these two loadbearing surfaces being in contact in a complementary way with one loadbearing surface (52) of the block (5) one, and with a loadbearing surface (32) of the internal face of the plate (3) not including block, for the other.

10 According to a particular aspect, the axis of symmetry (d52) of the convex loadbearing surface (52) of the block (5) forms a determined angle (a4) with an axis (d51) perpendicular to its surface (51) with contact of the plate (1) so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their external faces induces an incline (a5) of the plates with each other.

15 According to a particular aspect, at least one of the loadbearing surfaces (12, 52, 21, 23, 32) allowing articulation has a shape making up part of a sphere.

20 According to a particular aspect, the loadbearing surfaces of the two faces of the nucleus (2) have shapes making up parts of a sphere, the face presenting a concave loadbearing surface (21) having a radius greater than that of the face presenting a convex loadbearing surface (23).

25 According to a particular aspect, each of the plates (1, 3) includes on its external face one or more protruding parts with small section forming a bony anchoring, these protruding parts coming to be embedded or impacted in the surface of contiguous bony elements (V) under the effect of pressure, once the prosthesis is in position between two vertebrae or bony elements.

According to a particular aspect, one or more of the pieces of the prosthesis include accidents of shape, notches (7) or perforations likely to see a tool again to facilitate the extraction of said prosthesis.

According to a particular aspect, the plates (1, 3) are composed of an alloy with base of stainless steel with cobalt-chromium and the nucleus (2) has polyethylene base.

In the same spirit, the invention proposes instrumentation for inserting or fitting the prosthesis according to one of claims 1 to 15 characterized in that it comprises an insertion guide (9,93) including an internal channel (90) presenting an end in which certain edges or support edges (910, 920, 931, 932), protrude from the others along the longitudinal axis (d9) of the channel so as to be able to take the place of distraction tools of a known type previously used to increase the opening of the disc space, this channel (90) presenting an internal section capable of surrounding these same distraction tools while they maintain this opening, then allowing their extraction through said channel while said support edges (910, 920, 931, 932), for their part, preserve the opening of the disc space by replacing the distraction tools, then receiving and guiding the prosthesis (P) for insertion in this disc space.

According to a particular aspect, the internal channel (90) presents an approximately rectangular section or with a shape approximately complementary to the exterior profile of the prosthesis, taken in a section along the plane perpendicular to the direction of insertion.

According to a particular aspect, the support edges (931, 932) of insertion guide (93) form an extension of the channel (90) walls located on a plane containing the axis of the spinal column.

According to a particular aspect, the insertion guide (9) is formed from at least two elements (91, 92) separated along one or more planes parallel to the longitudinal axis (d9) of the channel, these parts each including at least one portion of the transverse section of the channel and being able to be

spread apart according to a determined angle (a9) and allowing the introduction and sliding of the prosthesis (P) in the channel.

According to a particular aspect, the internal surface of the channel (90) on its walls opposite external faces of the plates (1, 3) of the prosthesis 5 (P), includes at least one groove (913, 914) allowing the passage of protruding parts (8, 81) for anchoring provided by these plates during displacement of the prosthesis in this channel (90).

According to a particular aspect, the instrumentation comprises approach means (95) of the prosthesis capable of receiving the prosthesis 10 and of maintaining with it all the different components, these approach means (95) being able to be connected by interlocking means to the insertion guide (93) so as to present the prosthesis at the entrance of the channel (90) in a position appropriate for allowing its entrance into this channel (90).

15 According to a particular aspect, the instruments comprises insertion means, called impactor (96) of the prosthesis in the channel (90) of the insertion guide (93) then into the disc space, this impactor being guided by the support means (95) so as to be in contact with the prosthesis in its part opposite the entrance of the channel (90), this impactor (96) being able to 20 apply or transmit a pressure or repeated shocks to the prosthesis to cause its sliding in the channel, then its insertion in the disc space.

According to a particular aspect, the support means include two shafts (951, 952) connected by an axis to a assembling end (955), these shafts being able to be closed up to pinch the prosthesis (P) between them and to 25 maintain it so assembled, these two shafts each providing connection means to the guide for use (93), this connection then maintaining these two shafts closed up on the prosthesis.

It must be obvious for those skilled in the art that the present invention allows embodiments in numerous other specific forms without going far from 30 the field of application of the invention as claimed. As a result, the present

embodiments must be considered by way of illustration, but may be modified in the field defined by the scope of the attached claims, and the invention must not be limited to details given above.

**CLAIMS**

1. Intervertebral disc prosthesis device comprising at least three pieces, which pieces include a plate (1) called lower and a plate (3) called upper (3) producing around at least one intermediate part called nucleus (2), an articulation by support or sliding between loadbearing surfaces (12, 15, 5 21, 23, 32) of said pieces, one of these pieces including at least one protruding part or accident of shape cooperating with the shape of at least one other of said parts to form an stop limiting the possibilities of movement of the nucleus, characterized in that this stop operation uses at least one stop external to the loadbearing surfaces comprising at least one part (161, 10 163) protruding from at least one plate (1), located outside the loadbearing surface (12, 15) of said plate and including a face directed towards the interior of the prosthesis, this face cooperating with a peripheral part (6) of the nucleus (21, 23) situated outside its loadbearing surfaces (21, 23) and in which the surface is directed towards the exterior of the nucleus, to limit 15 displacements of the nucleus in translation or in rotation or both in a plane approximately transverse to the spinal column.

2. Device according to claim 1 characterized in that the loadbearing surfaces (21, 21a, 23) of the nucleus (2) in contact with the lower plate (1) and upper plate (3) present axes of symmetry (d21, d23, 20 respectively) forming between them a determined angle (a2) that is not zero, so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their external surfaces induces an incline (a3) of these plates with each other.

3. Device according to claims 1 to 2 characterized in that this 25 external stop limits the movements in rotation of the nucleus (2) relative to at least one plate (1) by contact between parts (6, 161, 163) supporting each

other by stop surfaces, this support being done along a direction approximately parallel to the normal of each of these stop surfaces.

4. Device according to claims 1 to 3 characterized in that the external stop includes a tongue (6) protruding from the nucleus (6) which 5 inserts in one of the plates (1) by confining this tongue (6) in a housing (162) delimited by pillars (161) protruding from the internal face of this same plate (1) or by a recess (66) separating this tongue into two arms encircling a pillar (163) protruding from the internal face of this same plate (1), the internal face of a plate being defined at that oriented on the side of the nucleus.

10 5. Device according to claims 1 to 4 characterized in that the end of at least one pillar (161, 162, 163) presents a section greater than its base, this enlargement of the pillar cooperating with the shape of the external stop tongue (6) of the nucleus (2) to limit the raising of this same nucleus relative to the plate (1) providing this pillar.

15 6. Intervertebral disc prosthesis device comprising at least three pieces, including a plate (1) called lower and a plate (3) called upper (3) producing around at least one intermediate part called nucleus (2) an articulation by support or sliding between loadbearing surfaces (12, 15, 21, 23, 32) of said pieces, one of these pieces including at least one protruding 20 part or accident of shape cooperating with the shape of at least one other of said parts to form an stop limiting the possibilities of movement of the nucleus, characterized in that the loadbearing surfaces (21, 21a, 23) of the nucleus (2) in contact with the lower plate (1) and upper plate (3) present axes of symmetry (d21, d23, respectively) forming between them a 25 determined angle (a2) to is not zero so that a pressure (F) exerted on the two plate (1, 3) along directions perpendicular to their external surfaces induces an incline (a3) of these plates with each other.

7. Device according to claim 6 characterized in that the function of the stop uses at least one stop external to the loadbearing surfaces comprising at least one part (161, 163) protruding from at least one plate (1) located outside the loadbearing surface (12, 15) of said plate and including a  
5 face directed towards the interior of the prosthesis, this face cooperating with a peripheral part (6) of the nucleus located outside its loadbearing surfaces (21, 23) and in which the surface is directed towards the exterior of the nucleus, to limit the displacements of the nucleus in translation or in rotation or both in a plane approximately transverse to the spinal column.

10 8. Device according to one of claims 1 to 6 characterized in that when the two plates have their external faces (10, 30) parallel to each other, their loadbearing surfaces (12, 12a, 32) cooperate with the loadbearing surfaces (21, 21a, 23) of the nucleus (2) present axes of symmetry (d<sub>12</sub>, d<sub>32</sub>) forming a determined angle (a<sub>4</sub>) between them so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their  
15 external surfaces induces an incline (a<sub>5</sub>) of these plates with each other.

9. Device according to one of claims 1 to 6 or according to claim 8 characterized in that the loadbearing surfaces (12, 32) provided by the internal face of the lower plate (1) and the internal face of the upper plate (3) are each in complementary contact with a supporting surface (21, 23,  
20 respectively) of the nucleus (2), and each present a shape, convex and concave, respectively, or inversely, this nucleus itself presenting a perimeter (20) approximately cylindrical along the axis of symmetry of its contact faces (21, 32).

25 10. Device according to one of claims 1 to 6 or 8 to 9 characterized in that the internal face of the lower plate (1) presents a loadbearing surface (12a) cooperating with a loadbearing surface (21a) of the lower face of the nucleus (2), this same nucleus including on its upper surface a convex loadbearing surface (23) in complementary contact with a concave

supporting surface (32) of the internal face of the upper plate (3) the loadbearing surface (12a) of the internal face of the lower plate being sufficiently extended to allow movement of the nucleus relative to this same lower plate.

5        11. Device according to one of claims 1 to 6 or 8 to 10 characterized in that an intermediate element called block (5) is added on the internal face of one (1) of the plates and produces an articulation with the other plate (3) around the nucleus (2) which nucleus presents a concave loadbearing surface (21) and a convex loadbearing surface (23) these two 10 loadbearing surfaces being in contact in a complementary way with one loadbearing surface (52) of the block (5) for one, and with a loadbearing surface (32) of the internal face of the plate (3) not including block, for the other.

15        12. Device according to claim 11 characterized in that the axis of symmetry (d52) of the convex loadbearing surface (52) of the block (5) forms a determined angle (a4) with an axis (d51) perpendicular to its surface (51) with contact of the plate (1) so that a pressure (F) exerted on the two plates (1, 3) along directions perpendicular to their external faces induces an incline (a5) of the plates with each other.

20        13. Device according to one of claims 1 to 6 or 8 to 12 characterized in that at least one of the loadbearing surfaces (12, 52, 21, 23, 32) allowing articulation has a shape making up part of a sphere.

25        14. Device according to one of claims 1 to 6 or 8 to 13 characterized in that the loadbearing surfaces of the two faces of the nucleus (2) have shapes making up parts of a sphere, the face presenting a concave loadbearing surface (21) having a radius greater than that of the face presenting a convex loadbearing surface (23).

15. Device according to one of claims 1 to 6 or 8 to 14 characterized in that each of the plates (1, 3) includes on its external face one or more protruding parts with small section forming a bony anchoring, these protruding parts coming to be embedded or impacted in the surface of 5 contiguous bony elements (V) under the effect of pressure, once the prosthesis is in position between two vertebrae or bony elements.

16. Device according to one of claims 1 to 6 or 8 to 15 characterized in that one or more of the pieces of the prosthesis include accidents of shape, notches (7) or perforations likely to see a tool again to 10 facilitate the extraction of said prosthesis.

17. Device according to one of claims 1 to 6 or 8 to 16 characterized in that the plates (1, 3) are composed of an alloy with base of stainless steel with cobalt-chromium and the nucleus (2) has polyethylene base.

15 18. Instrumentation device for inserting or fitting the prosthesis according to one of claims 1 to 17 characterized in that it comprises an insertion guide (9,93) including an internal channel (90) presenting an end in which certain edges, or support edges (910, 920, 931, 932), protrude from the others along the longitudinal axis (d9) of the channel so as to be able to 20 take the place of distraction tools of a known type previously used to increase the opening of the disc space, this channel (90) presenting an internal section capable of surrounding these same distraction tools while they maintain this opening, then allowing their extraction through said channel while said support edges (910, 920, 931, 932), for their part, 25 preserve the opening of the disc space by replacing the distraction tools, then receiving and guiding the prosthesis (P) for insertion in this disc space.

19. Instrumentation device for fitting the prosthesis according to claim 18 characterized in that the internal channel (90) presents a

approximately rectangular cross section or with a shape approximately complementary to the exterior profile of the prosthesis, taken in a section along the plane perpendicular to the direction of insertion.

20. Instrumentation device for fitting the prosthesis according to  
5 one of claims 18 to 19 characterized in that the support edges (931, 932) of  
insertion guide (93) form an extension of the channel (90) walls located on a  
plane containing the axis of the spinal column.

21. Instrumentation device for fitting the prosthesis according to  
one of claims 18 to 20 characterized in that the insertion guide (9) is formed  
10 from at least two elements (91, 92) separated along one or more planes  
parallel to the longitudinal axis (d9) of the channel, these parts each  
including at least one portion of the transverse section of the channel and  
being able to be spread apart according to a determined angle (a9) and  
allowing the introduction and sliding of the prosthesis (P) in the channel.

15 22. Instrumentation device for fitting the prosthesis according to  
one of claims 18 to 21 characterized in that the internal surface of the  
channel (90) on its walls opposite external faces of the plates (1, 3) of the  
prosthesis (P), includes at least one groove (913, 914) allowing the passage  
of protruding parts (8, 81) for anchoring provided by these plates during  
20 displacement of the prosthesis in this channel (90).

23. Instrumentation device for fitting the prosthesis according to  
one of claims 18 to 22 characterized in that it comprises approach means  
(95) of the prosthesis capable of receiving the prosthesis and of maintaining  
with it all the different components, these approach means (95) being able to  
25 be connected by interlocking means to the insertion guide (93) so as to  
present the prosthesis at the entrance of the channel (90) in a position  
appropriate for allowing its entrance into this channel (90).

24. Instrumentation device for fitting the prosthesis according to one of claims 18 to 23 characterized in that it comprises insertion means, called impactor (96) of the prosthesis in the channel (90) of the insertion guide (93) then into the disc space this impactor being guided by the support means (95) so as to be in contact with the prosthesis in its part opposite the entrance of the channel (90), this impactor (96) being able to apply or transmit a pressure or repeated shocks to the prosthesis to cause its sliding in the channel then its insertion in the disc space.

25. Instrumentation device for fitting the prosthesis according to one of claims 18 to 24 characterized in that the support means include two shafts (951, 952) connected by an axis to an assembling end (955), these shafts being able to be closed up to pinch the prosthesis (P) between them and to maintain it so assembled, these two shafts each providing connection means to the guide for use (93), this connection then maintaining these two shafts closed up on the prosthesis.

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fig. 1

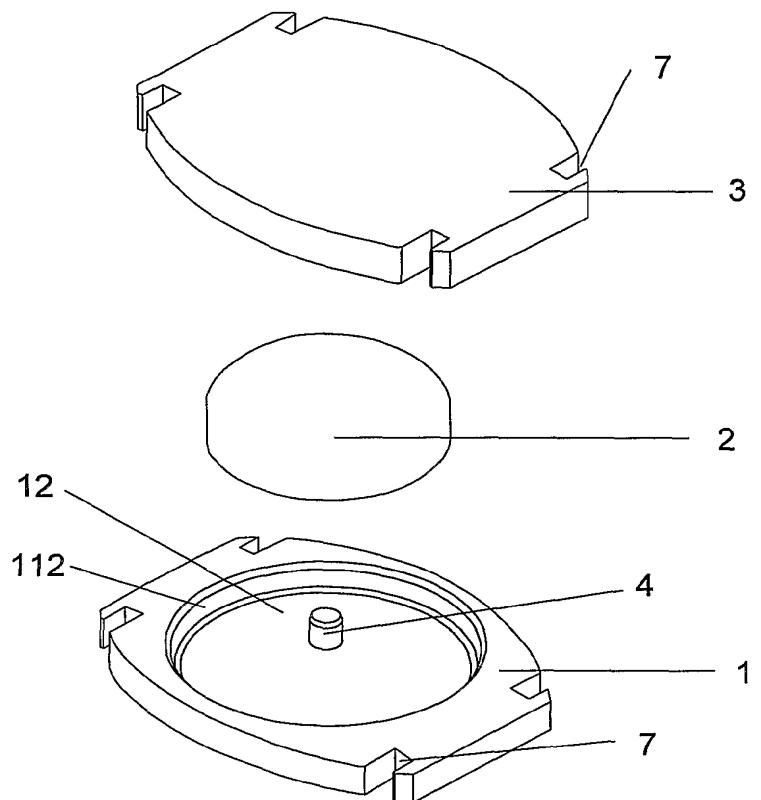
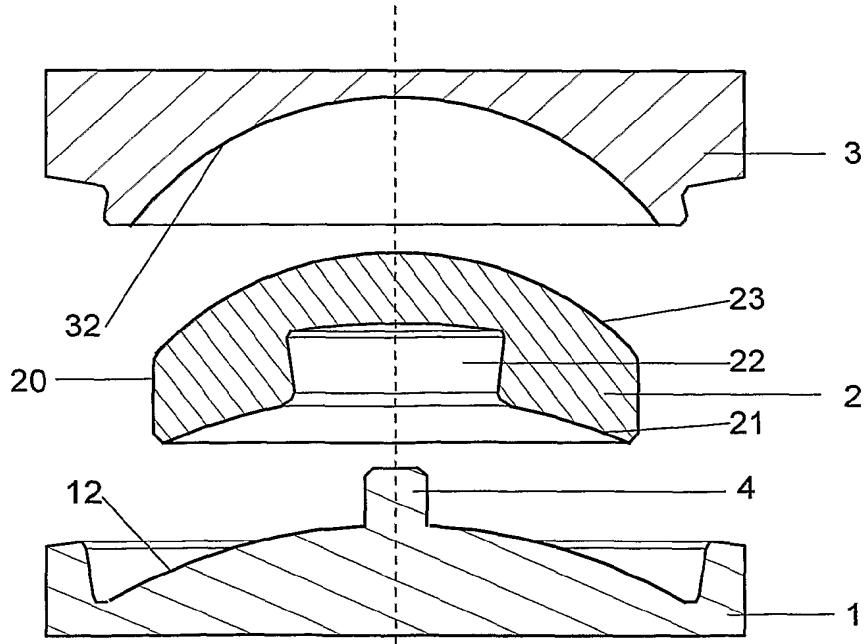


fig. 2



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fig. 3

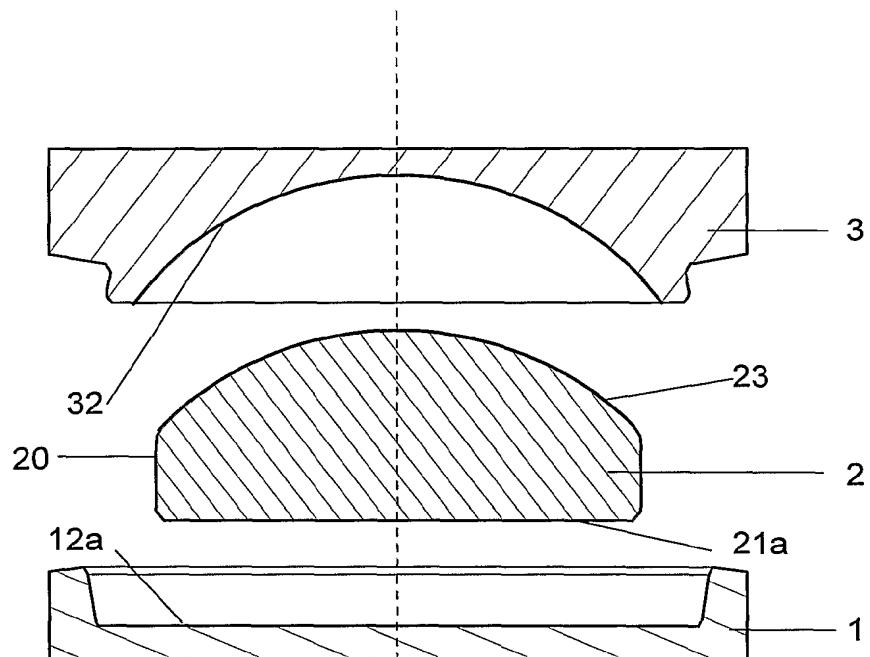
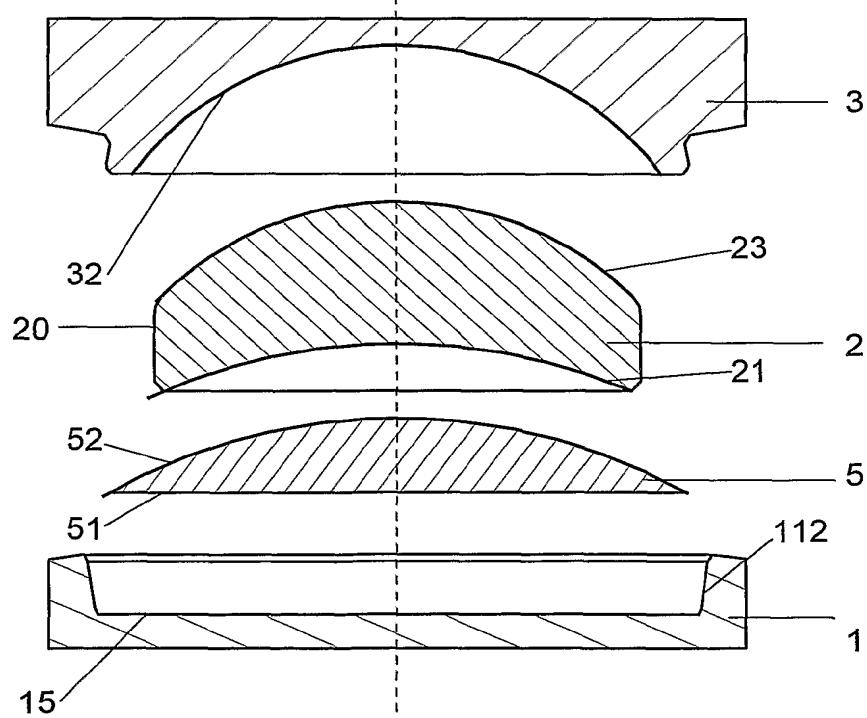


fig. 4



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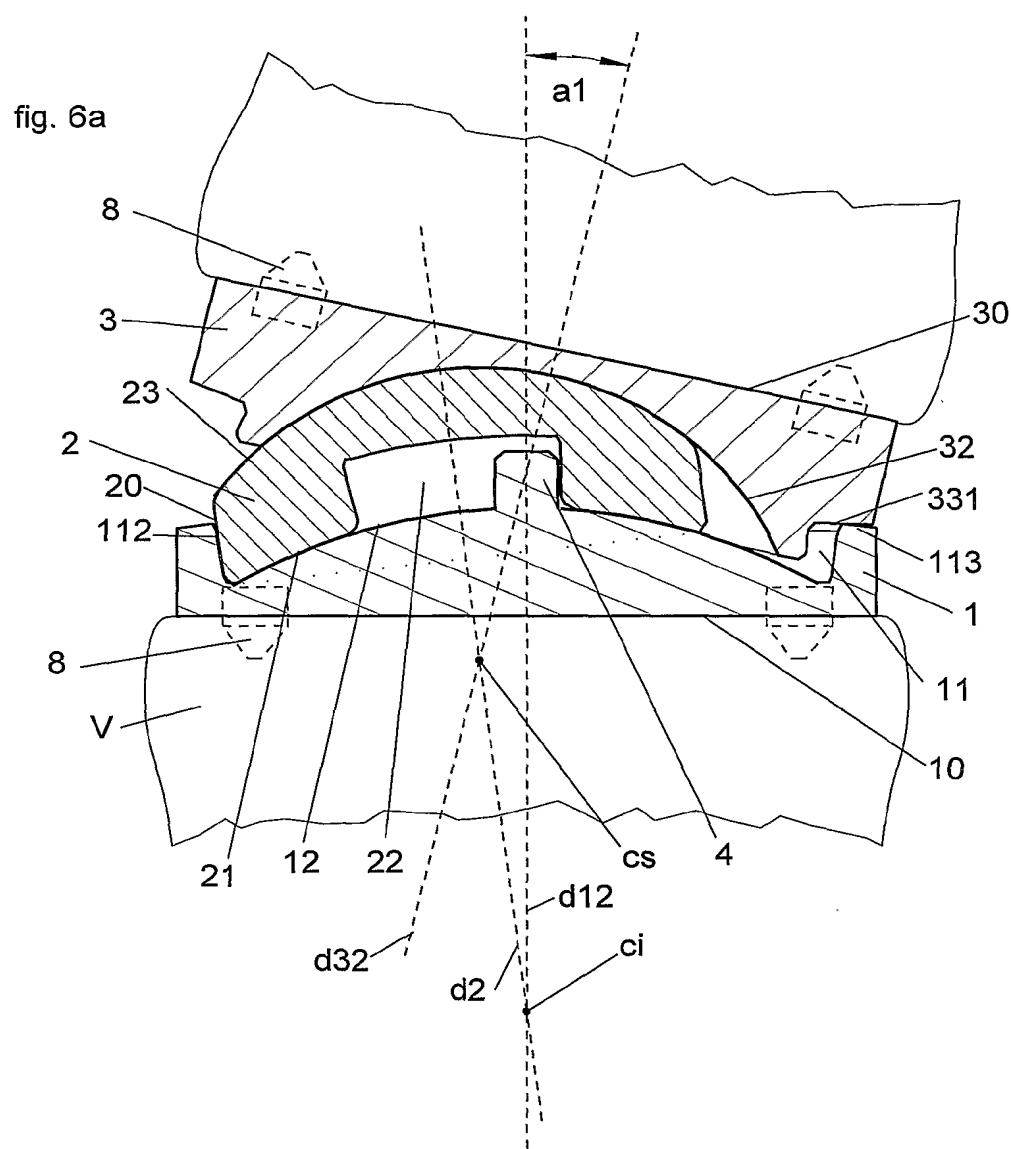


fig. 6b

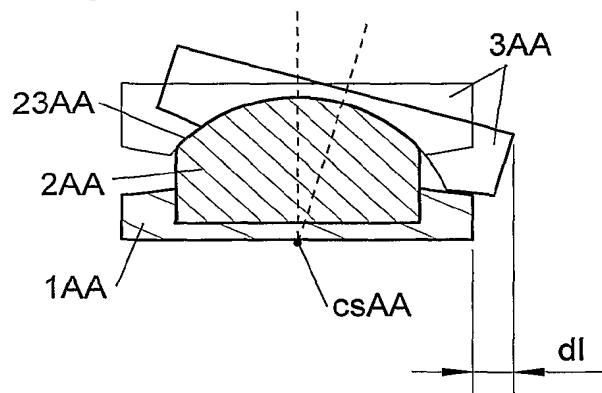
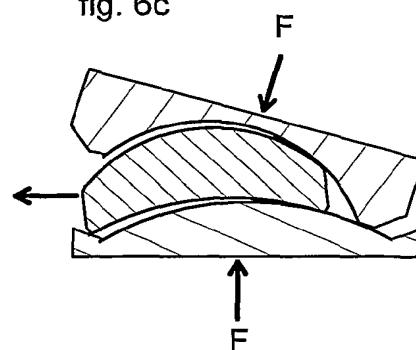


fig. 6c



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fig. 5

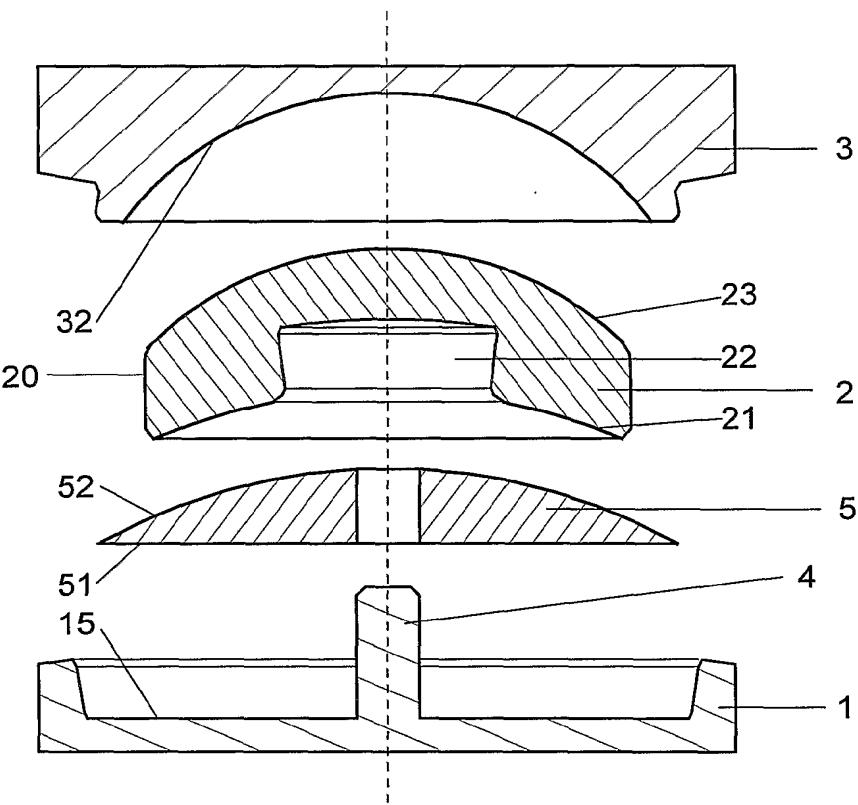
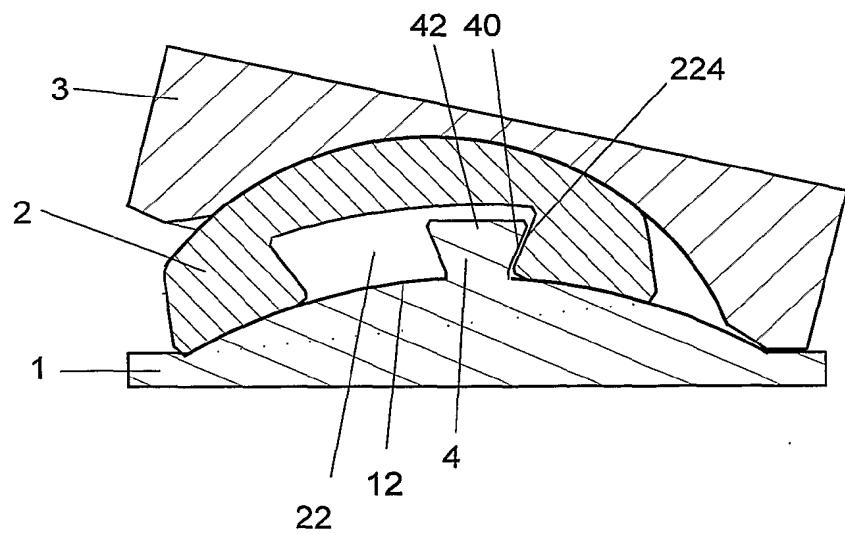


fig. 7



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fig. 8a

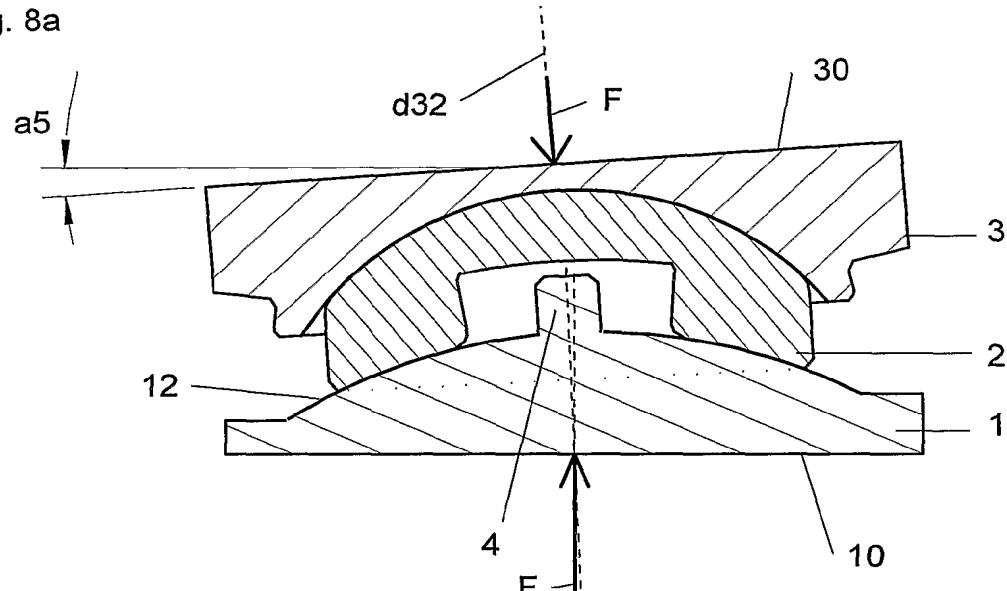
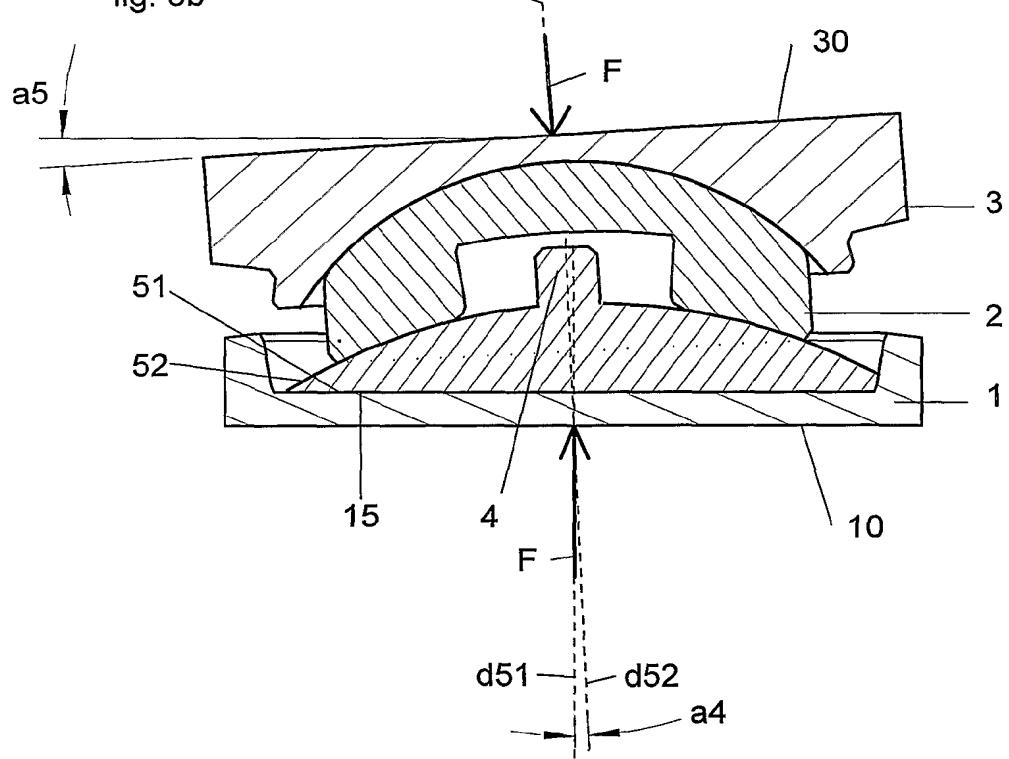
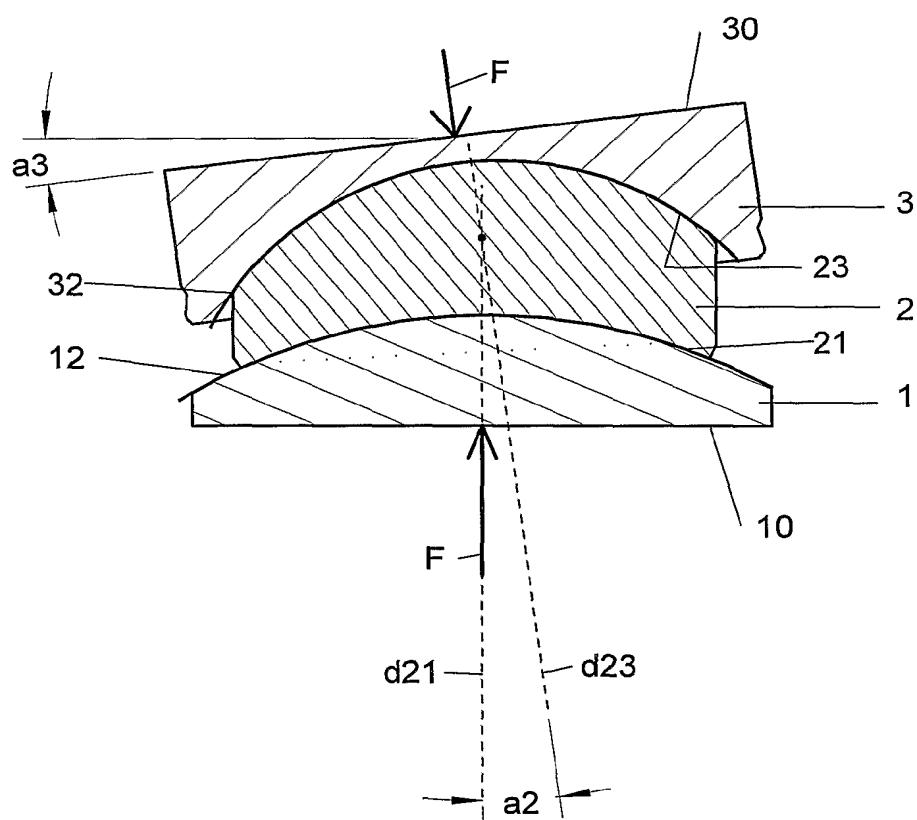


fig. 8b



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fig. 8c



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fig. 9a

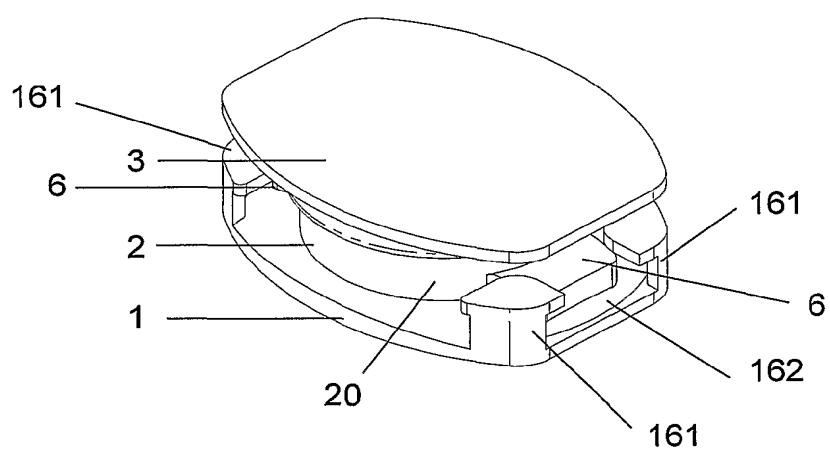
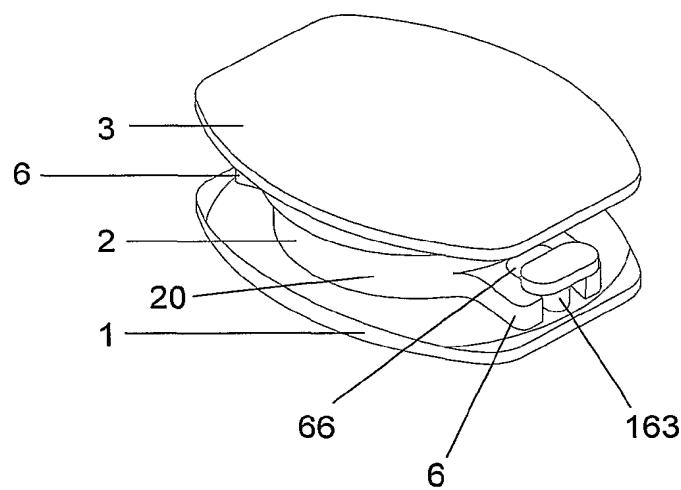


fig. 9b



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fig. 10

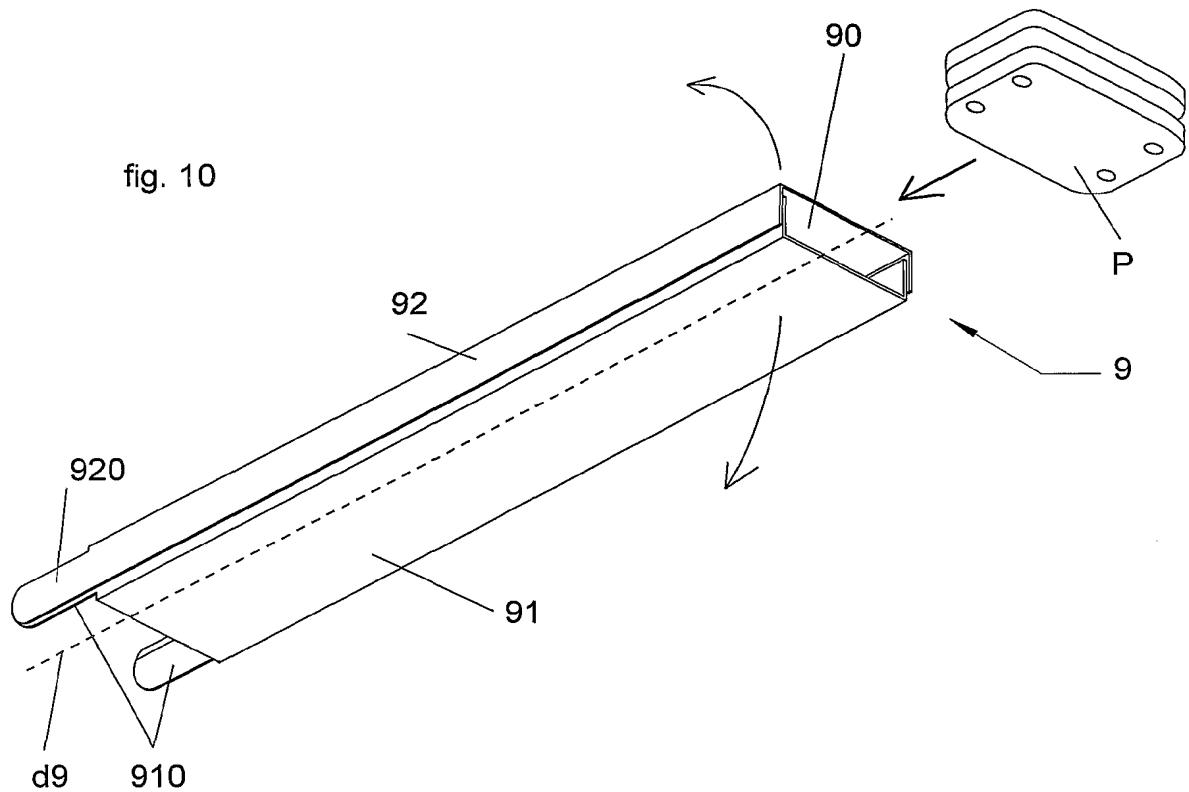
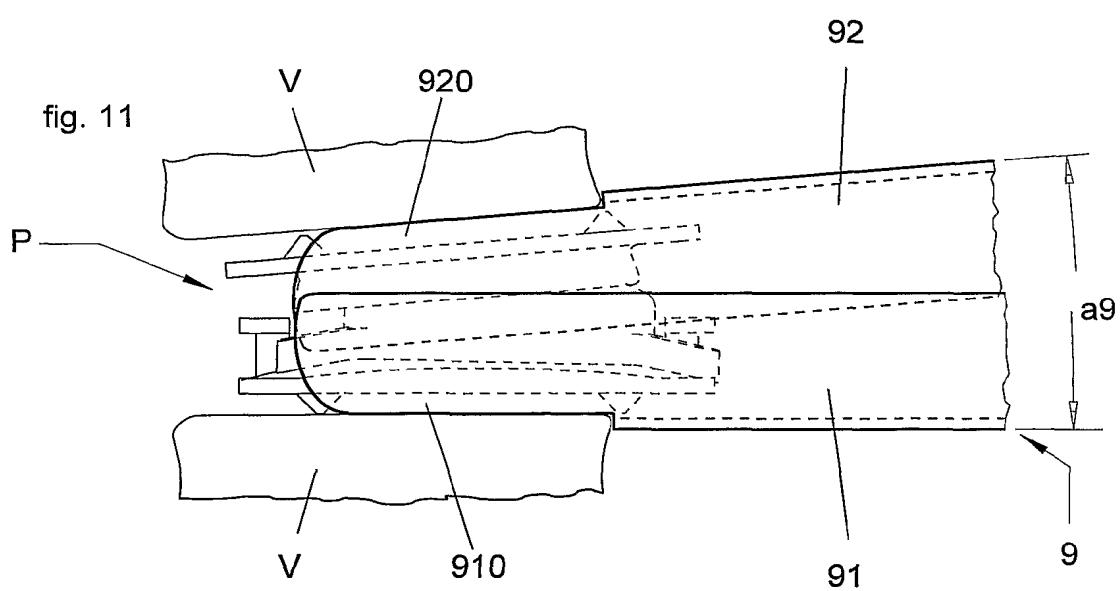


fig. 11



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fig. 12a

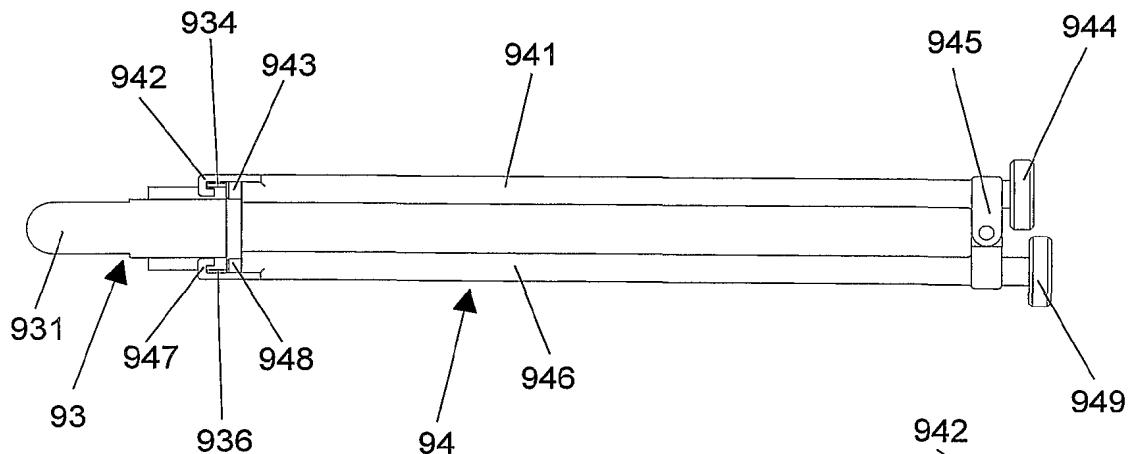
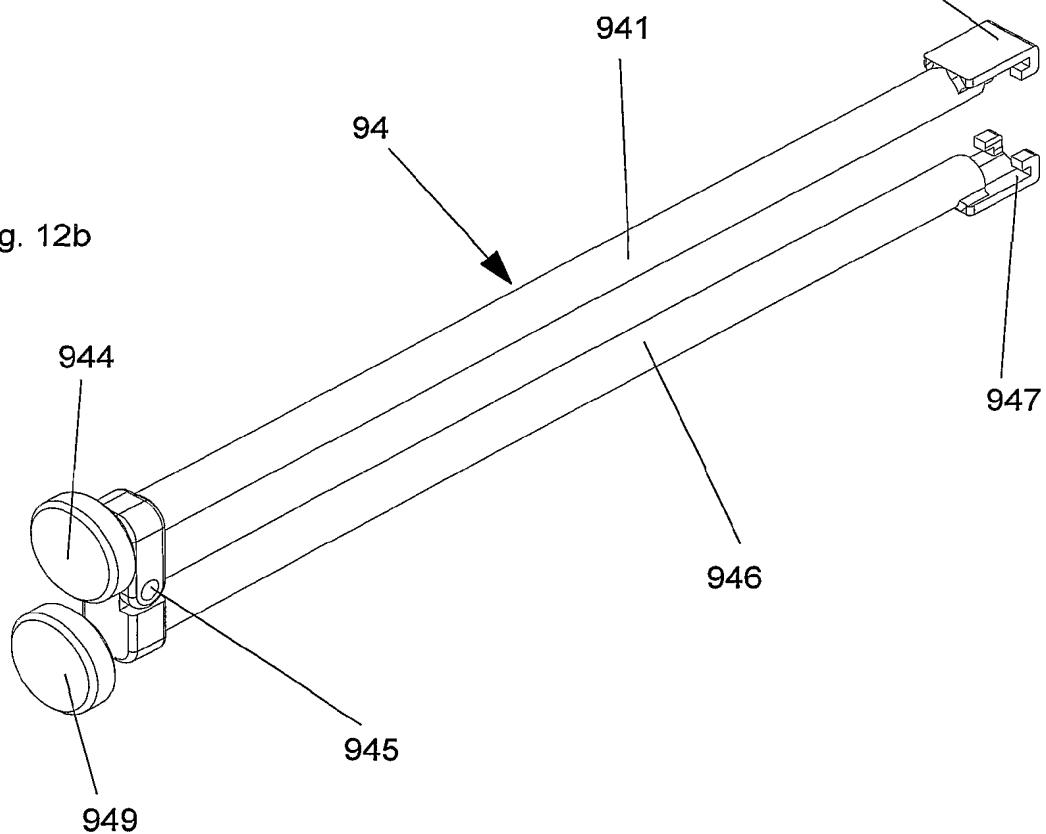


fig. 12b



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fig. 13

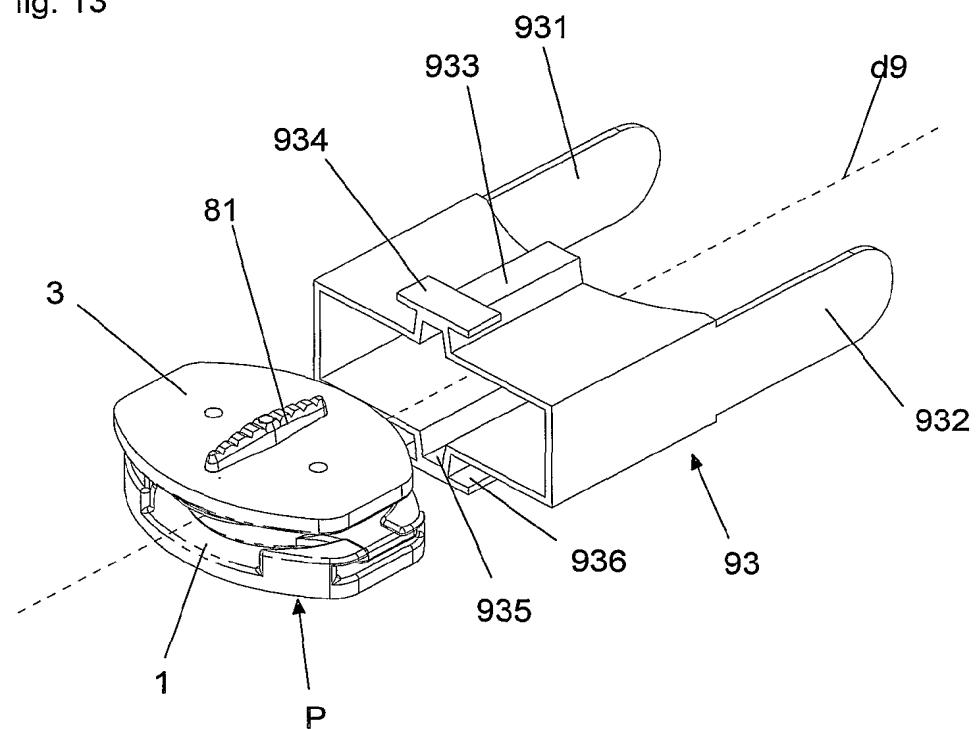


fig. 14

